# Human Muscle Force Modeling for Enhanced Assistive Device Control

Laura Hallock Ruzena Bajcsy BAIR/CPAR/BDD Internal Weekly Seminar 2018.10.26





There are many mechanically sophisticated, biomimetic devices on the market ...



UW "Highly Biomimetic Anthropomorphic Robotic Hand"



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PISA-IIT Softhand

Ottobock Bebionic hand







Gifu Hand III

There are many mechanically sophisticated, biomimetic devices on the market ...



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#### There are m **CHALLENGE** How can a human user control many degrees of freedom? NASA Robonaut hand Ottobock Bebionic hand GH Gifu Hand III DLR Hand II **PISA-IIT Softhand** ... but we don't know how to **control** them.

There are m

#### CHALLENGE

How can a human user control many degrees of freedom?

#### **KEY IDEA**

If we can **measure the output force of each muscle**, we should be able to **control an external device of the same complexity**.



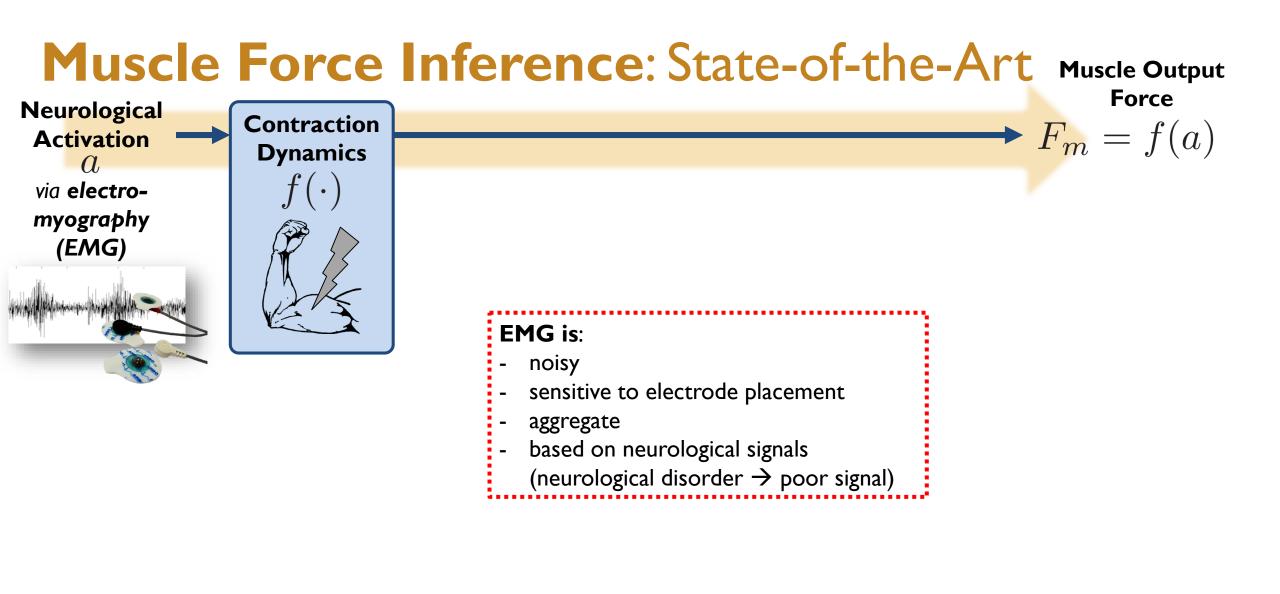
PISA-IIT Softhand

... but we don't know how to **control** them.

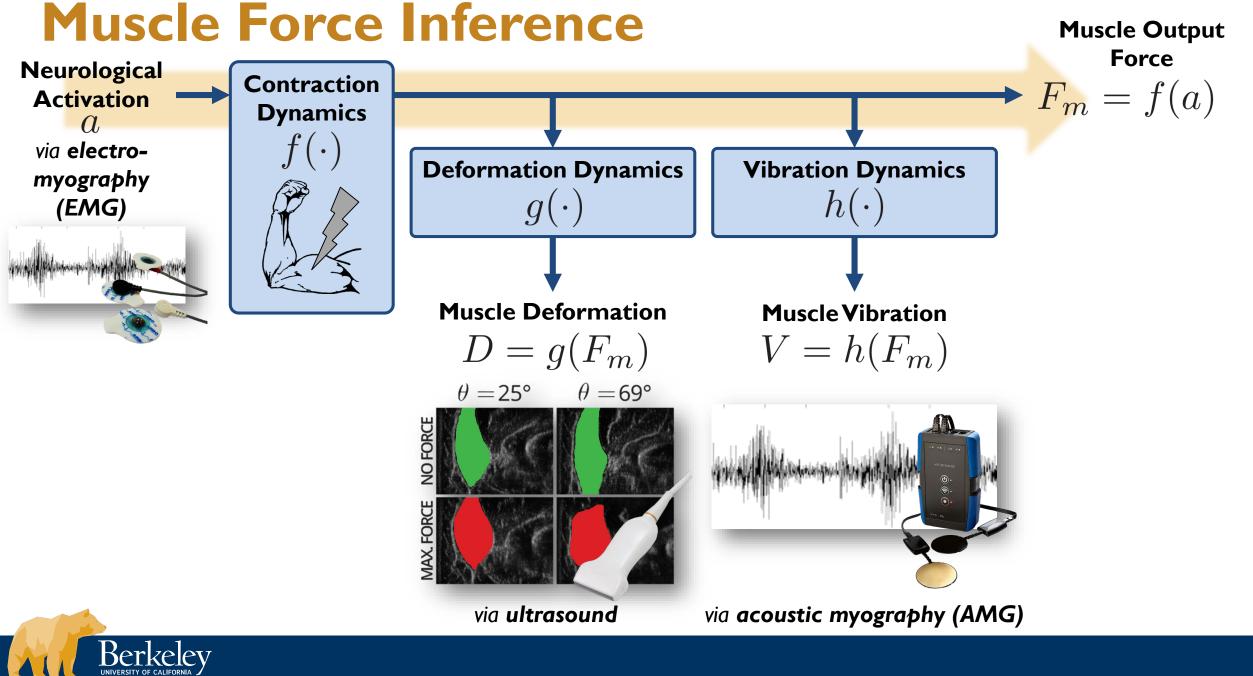
NASA Robonaut hand











#### Muscle Force Inference: Our Approach **Muscle Output** Force Neurological Contraction $\blacktriangleright F_m = f(a)$ Activation **Dynamics** $= g^{-1}(D)$ via electro-**Deformation Dynamics Vibration Dynamics** $= h^{-1}(V)$ myography $g(\cdot)$ $h(\cdot)$ (EMG) **Muscle Deformation** Muscle Vibration $V = h(F_m)$ $D = g(F_m)$ Both deformation and vibration $\theta = 25^{\circ}$ $\theta = 69^{\circ}$ are **mechanical signals**, allowing for measurement of muscle force **without** considering the neurological feedback loop. (Until we want to explicitly study it!) via **ultrasound** via acoustic myography (AMG)

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#### Muscle Force Inference: Our Approach **Muscle Output** Force Neurological Contraction $\blacktriangleright F_m = f(a)$ Activation **Dynamics** $= g^{-1}(D)$ via electro-**Deformation Dynamics Vibration Dynamics** $= h^{-1}(V)$ myography $g(\cdot)$ (EMG) **Muscle Deformation Muscle Vibration** $D = g(F_m)$ $V = h(F_m)$ Both deformation and vibration $\theta = 25^{\circ}$ $\theta = 69^{\circ}$ are **mechanical signals**, allowing for measurement of Warmen it muscle force **without** Deformation signal is **highly** considering the neurological localized! feedback loop. (Until we want to explicitly study it!) via **ultrasound** via acoustic myography (AMG)

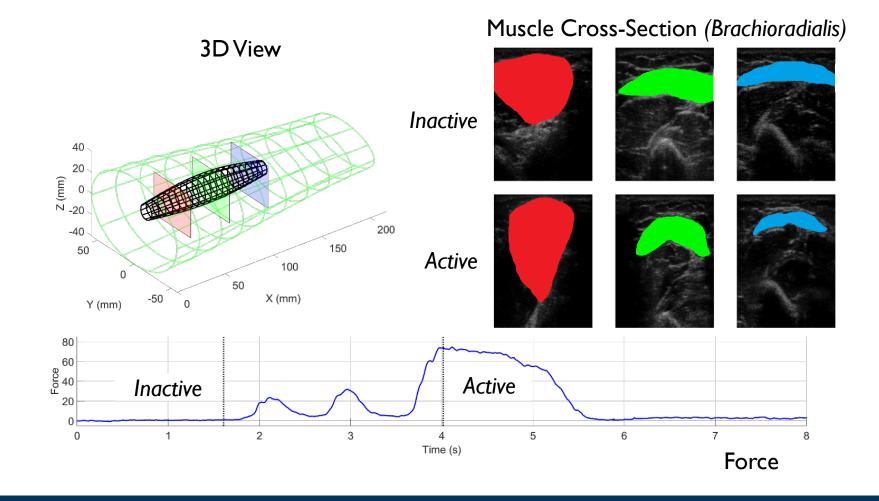
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#### **Deformation Modeling Challenges**

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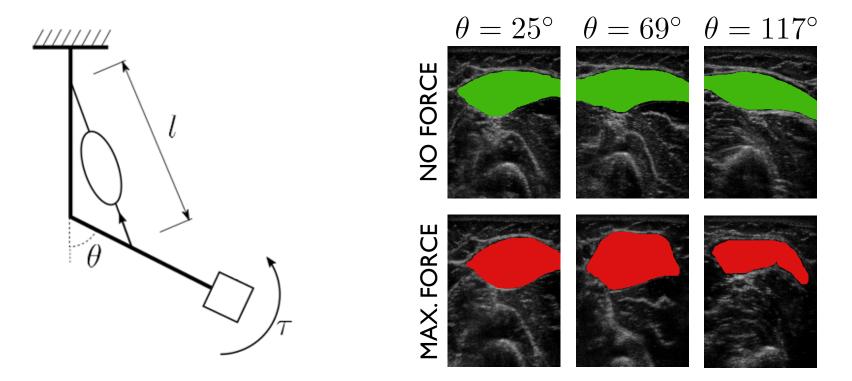
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I. Observed deformation varies substantially with sensor location.



#### **Deformation Modeling Challenges**

- I. Observed deformation varies substantially with sensor location.
- 2. Deformation occurs under changes in both kinematic configuration and force output.





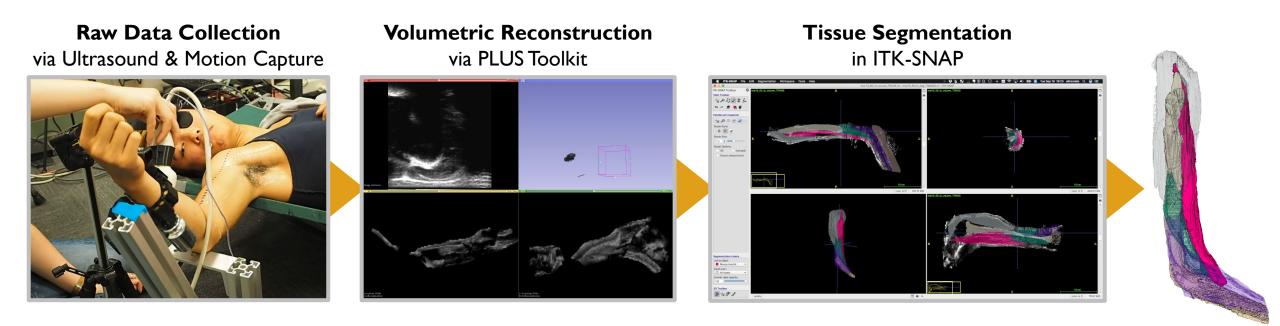
#### **Deformation Modeling Challenges**

- I. Observed deformation varies substantially with sensor location.
- 2. Deformation occurs under changes in both kinematic configuration and force output.

To build a model that can robustly infer muscle force, we need to observe the **entire muscle** under **multiple** (ideally, factorial) **joint positions** and **loading conditions**.



# Approach: Ultrasound + Motion Capture



Using **motion capture** to track the **ultrasound probe position**, we can generate **full 3D scans** of the arm under **static conditions**.

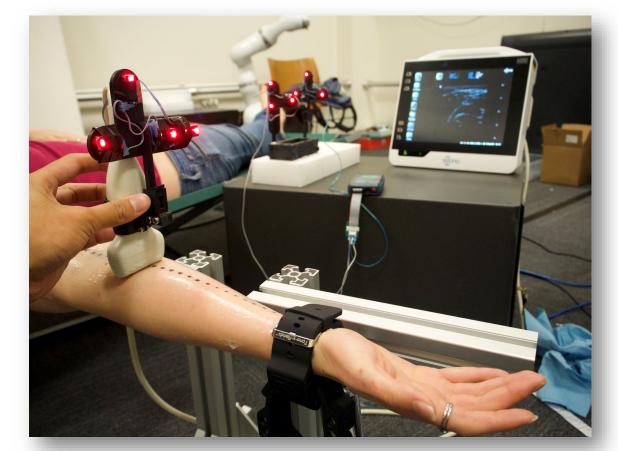


# **Approach:** Data Selection

**Model target**: elbow flexors (biceps brachii, brachialis, brachioradialis)

Data set:

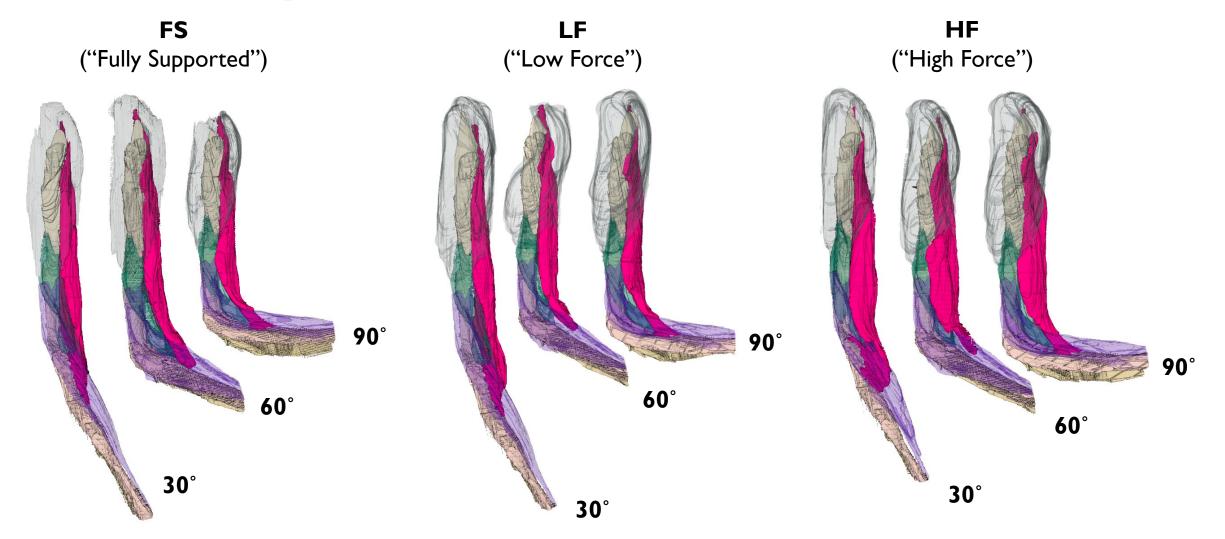
- 3 subjects (1 F, 2 M)
- full arm ultrasound volumetric scan
- 4 elbow flexion angles, 0–90°
- 5 loading conditions
  - **FS**: fully supported
  - GC: gravity compensation only
  - LF: light wrist weight (~225g)
  - **MF**: medium wrist weight (~725g)
  - HF: heavy wrist weight (~950g)



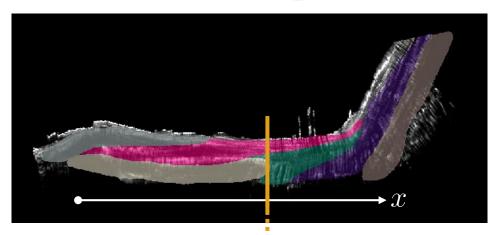
Ultrasound volumetric data collection, HART Lab 2017

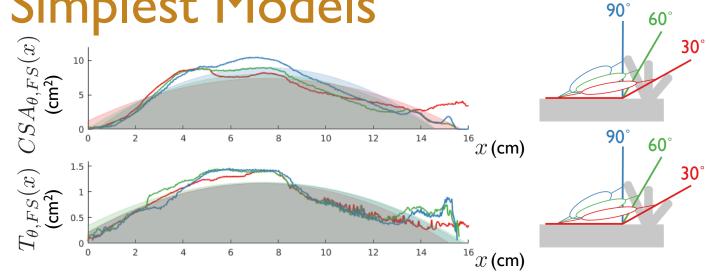


#### Preliminary Results: Qualitative





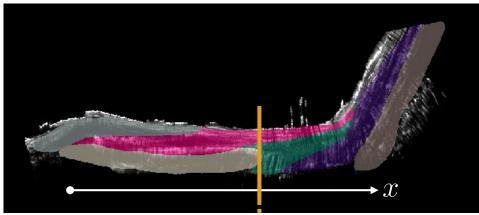


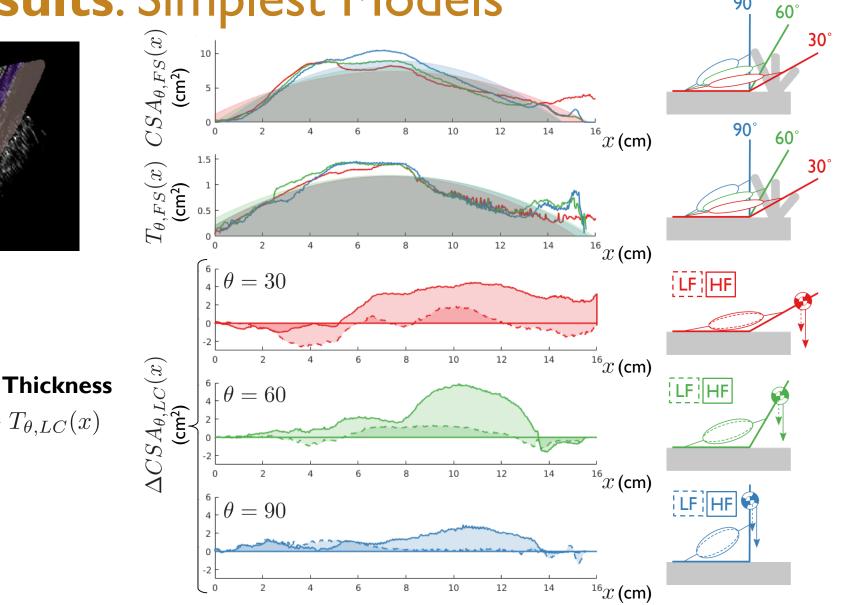


#### Cross-Sectional Area $CSA_{\theta,LC}(x)$ Thickness $T_{\theta,LC}(x)$ $T_{\theta,LC}(x)$

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#### 17





**Cross-Sectional** Area

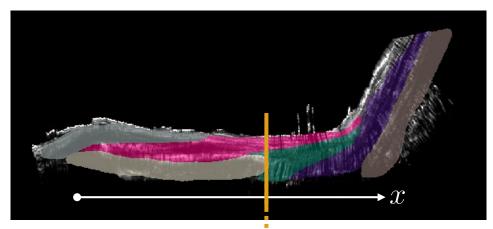
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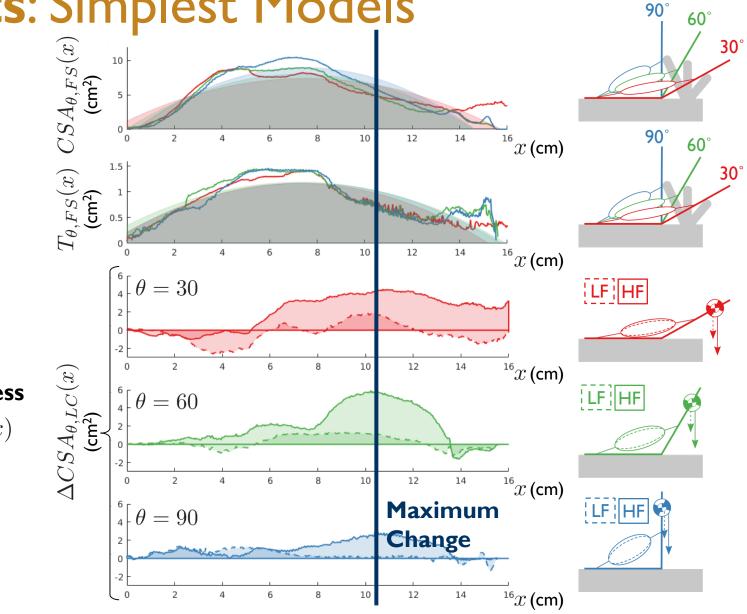
 $CSA_{\theta,LC}(x)$ 



Biceps Cross-Section

**90**°





**Cross-Sectional** Area

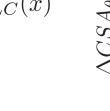
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 $CSA_{\theta,LC}(x)$ 

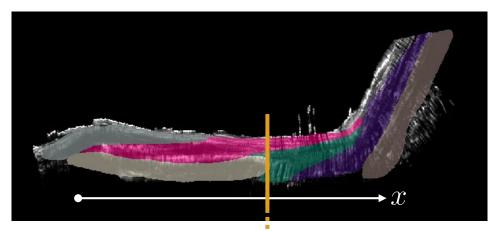


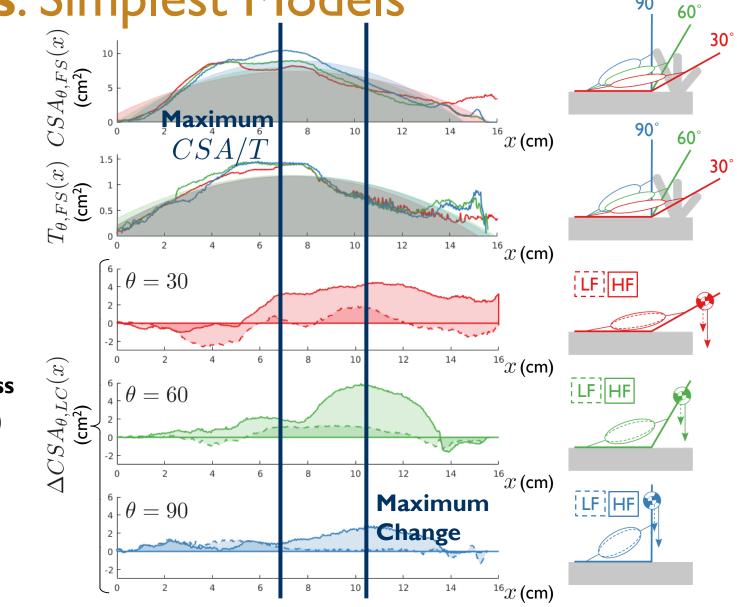
Biceps Cross-Section

Thickness  $T_{\theta,LC}(x)$ 









**Cross-Sectional** 

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Area  $CSA_{\theta,LC}(x)$ 



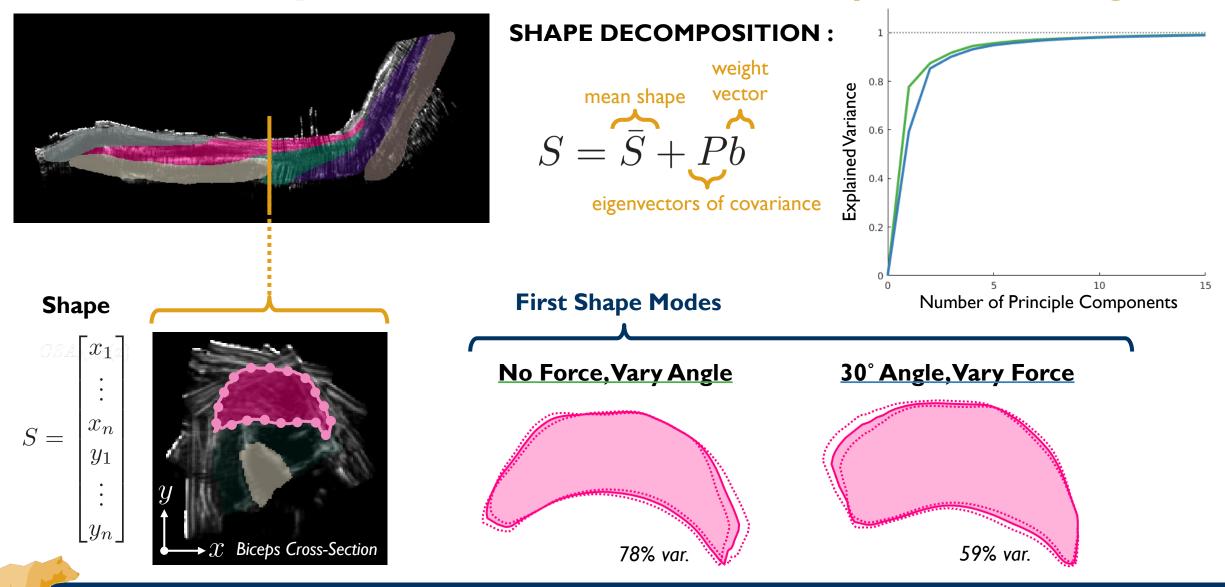
Biceps Cross-Section

Thickness  $T_{\theta,LC}(x)$ 

20

**90**°

#### Preliminary Results: Statistical Shape Modeling



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### Current / Future Work: Big Questions

- Translational: If we measure kinematic configuration using other sensors (e.g., motion capture), can we infer a clean relationship between force and deformation that can be used as a control signal?
- Basic: Can these muscle force measures be used to build better models of neuromuscular contraction dynamics and better interpret {EMG, fMRI, EEG, etc.} signals?



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L.A. Hallock, A. Kato, and R. Bajcsy. "Empirical Quantification and Modeling of Muscle Deformation: Toward Ultrasound-Driven Assistive Device Control." *IEEE International Conference on Robotics and Automation (ICRA)*, 2018.

L.A. Hallock and R. Bajcsy. "A Preliminary Evaluation of Acoustic Myography for Real-Time Muscle Force Inference." International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC), 2018. (late-breaking report)

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